Whole brain resting state functional connectivity abnormalities in schizophrenia

Archana Venkataramana, Thomas J. Whitforda,b, Carl-Fredrik Westina,c, Polina Gollanda, Marek Kubickiad,⁎

a Computer Science and Artificial Intelligence Laboratory, Massachusetts Institute of Technology, Cambridge, MA, United States
b Melbourne Neuropsychiatry Centre, Department of Psychiatry, University of Melbourne and Melbourne Health, Australia
c Laboratory for Mathematical Imaging, Harvard Medical School, Boston, MA, United States
d Psychiatry Neuroimaging Laboratory, Department of Psychiatry, Brigham and Women’s Hospital, Harvard Medical School, United States

A R T I C L E   I N F O

Article history:
Received 17 February 2012
Received in revised form 26 April 2012
Accepted 30 April 2012
Available online 26 May 2012

Keywords:
Functional connectivity
Schizophrenia
Positive and negative symptoms

A B S T R A C T

Background: Schizophrenia has been associated with disturbances in brain connectivity; however the exact nature of these disturbances is not fully understood. Measuring temporal correlations between the functional MRI time courses of spatially disparate brain regions obtained during rest has recently emerged as a popular paradigm for estimating brain connectivity. Previous resting state studies in schizophrenia explored connections related to particular clinical or cognitive symptoms (connectivity within a-priori selected networks), or connections restricted to functional networks obtained from resting state analysis. Relatively little has been done to understand global brain connectivity in schizophrenia.

Methods: Eighteen patients with chronic schizophrenia and 18 healthy volunteers underwent a resting state fMRI scan on a 3 T magnet. Whole brain temporal correlations have been estimated using resting-state fMRI data and free surfer cortical parcellations. A multivariate classification method was then used to indentify brain connections that distinguish schizophrenia patients from healthy controls.

Results: The classification procedure achieved a prediction accuracy of 75% in differentiating between groups on the basis of their functional connectivity. Relative to controls, schizophrenia patients exhibited co-existing patterns of increased connectivity between parietal and frontal regions, and decreased connectivity between parietal and temporal regions, and between the temporal cortices bilaterally. The decreased parieto-temporal connectivity was associated with the severity of patients’ positive symptoms, while increased fronto-parietal connectivity was associated with patients’ negative and general symptoms.

Discussion: Our analysis revealed two co-existing patterns of functional connectivity abnormalities in schizophrenia, each related to different clinical profiles. Such results provide further evidence that abnormalities in brain connectivity, characteristic of schizophrenia, are directly related to the clinical features of the disorder.

© 2012 Elsevier B.V. All rights reserved.

1. Introduction

Schizophrenia is a devastating disorder that simultaneously affects multiple cognitive domains including language, memory, attention and executive functioning. Since each of these functions relies on efficient communication between several, often distant, brain regions, schizophrenia has been hypothesized to arise from disruptions in brain connectivity (Konrad and Winterer, 2008). Based on the clinical symptoms, lesion studies and initial in vivo MRI studies, it has been predicted that such abnormalities should affect frontal, temporal and parietal regions, and their connections (Kraepelin, 1919/1971; Weinberger et al., 1992; McGuire and Frith, 1996). Since the emergence of functional MRI (fMRI), many studies have investigated functional neuroanatomy and the correlates of the cognitive dysfunctions observed in schizophrenia (Niznikiewicz et al., 2003). However, these studies are limited by several factors, one of them being the low Signal-to-Noise Ratio (SNR), typical of fMRI data derived during experiments involving cognitive tasks, forcing the interpretations of such studies to be based on aggregated data of 10 or more subjects, rather than a single individual. Another factor limiting the clinical application of fMRI is the issue of task difficulty, where participants are limited to those able to perform a given task, and hence, whose cognition is least affected by the disease (Greicius, 2008). An additional difficulty comes with using fMRI data to compare populations, where matching for cognitive performance might lead to removing the data variance due to disease related cognitive decline (Greicius, 2008).

Resting-state fMRI is a relatively new functional imaging method, with the potential to overcome most of the above limitations. I.e. since no cognitive task is involved, there is no need to correct for cognitive performance, or exclude subjects that cannot perform the task (thus biasing the sample). Resting-state functional MR data is collected in the absence of any experimental task; the subject is asked to rest quietly, either with their eyes closed or with their eyes opened and fixating on one point. Initial experiments suggest that various regions of the brain remain active during this process, expressed in low frequency BOLD fluctuations. It is believed that temporal correlations between

⁎ Corresponding author at: Psychiatry Neuroimaging Laboratory, 1249 Boylston Street-3rd Floor, Boston, MA 02215, United States. Tel.: +1 617 525 6117; fax: +1 617 525 6150.
E-mail address: kubicki@bwh.harvard.edu (M. Kubicki).
these fluctuations reveal the intrinsic functional organization of the brain (Biswal et al., 1995; Gusnard and Raichle, 2001; Peltier et al., 2003). Univariate tests and random effects analysis are, to a great extent, the standard in population studies of functional connectivity (Liang et al., 2006; Greicius et al., 2007; Zhou et al., 2007). Using these methods several “resting state networks (RSNs)” can be robustly identified (Beckmann et al., 2005). The method has been also applied to several brain disorders, including Alzheimer’s, depression, schizophrenia, ADHD and multiple sclerosis (MS). While results of studies in Alzheimer’s are consistent and encouraging, the same is not true for schizophrenia (Greicius, 2008). Several studies describe increased connectivity within the default mode network (one of the most robust of the resting state networks (Zhou et al., 2007; Whitfield-Gabrieli et al., 2009), while others report decreased connectivity within this network (Bluhm et al., 2007; Zhou et al., 2010). Reports on changes in correlations between other RSNs are inconsistent as well (Zhou et al., 2007; Bluhm et al., 2007).

As stated previously, schizophrenia is a multi-dimensional disease, where several separate, but interrelated cognitive domains and processes appear to be affected (Kalkstein et al., 2010). Thus, the clinical symptoms of schizophrenia are most likely not related to any particular brain region brain connection, but rather appear due to instability of communication within and between networks of regions, across the spectrum of cognitive domains. Resting state fMRI data has a potential to map those interactions and their abnormalities in schizophrenia. However, traditional functional connectivity analysis focuses on disruptions of single connections or single cognitive networks, and interactions between them are often ignored, leaving the models and clinical hypotheses that are being tested much too simplified. Specifically, most functional connectivity studies of schizophrenia use t-scores/p-values to identify the significant connections. We believe there are two issues with this approach: (1) the tests are done independently on each connection, and therefore one cannot identify networks of connections that together cause abnormalities, and (2) t-scores/p-values are not necessarily good measures of the relevance of specific connections. Only recently have the multivariate classifier and regression approaches been used successfully in population based functional connectivity analyses (in depression (Craddock et al., 2009), and brain development (Dosenbach et al., 2010)). In this paper, we use a similar multivariate classifier approach (Random Forest classification (Breiman, 2001)). The method has been introduced, and described in detail, including its comparison to univariate tests in Venkataraman et al. (2010). We address the above-mentioned limitations of univariate approaches by using a multi-pattern score to select the relevant features (Gini importance), and by using prediction as the primary way to validate the results (i.e., can the model predict the diagnosis of a new subject).

Here, we applied the method to the data collected from patients with chronic schizophrenia and their matched healthy controls, intending to identify and characterize patterns of brain connectivities that can differentiate patients with schizophrenia and healthy controls. Based on schizophrenia literature as well as our previous studies, we hypothesized that the connections/networks best predicting schizophrenia diagnosis will involve fronto-temporal connections, at least partially overlapping with the default network. We further expected that the patterns of both hyper as well as hypo connectivity will be represented in schizophrenia.

2. Methods

2.1. Subjects

Eighteen male patients diagnosed with chronic schizophrenia (SZ) (using DSM-IV criteria based on SCID-P interviews and a review of the medical records), and 18 male healthy volunteers (NC) were matched on gender, handedness, parental socio-economic status (PSES), age and premorbid IQ. All subjects gave written informed consent prior to participation in the study, and the study was approved by an institutional IRB. Subjects were included in the study if they fulfilled the following criteria: right-handedness, aged between 18 and 55, no neurological illness, no alcohol or drug dependence in the last 5 years and no abuse in the past year. Healthy control subjects were additionally screened to exclude first-degree relatives with an Axis I disorder. We used the Positive and Negative Syndrome Scale (PANSS (Kay et al., 1987)) to investigate the functional role of brain connections in clinical abnormalities in schizophrenia. Demographic data is included in Table 1. At the time of the scan, the majority of patients were on medication. Daily chlorpromazine equivalent antipsychotic dosage (Woods, 2003) was 356.5 ± 291.7 mg, and the content of the medication was as follows: typical antipsychotic, 7.4%, atypical antipsychotic, 70.4%, both, 11.1%, and unmededicated at the scan time, 11.1%.

2.2. Imaging data acquisition

Imaging was performed using a 3-T whole body MRI Echospeed system (General Electric Medical Systems, Milwaukee, WI). Two sets of data were collected: structural MRI, used for brain parcelation, and resting state fMRI, used for functional connectivity analysis. All images were collected during one imaging session with 8 Channel coil and ASSET (Array Spatial Sensitivity Encoding techniques, GE) with a SENSE factor (speed-up) of 2. The structural MRI acquisition included two MRI pulse sequences: spoiled gradient-recalled acquisition (fastSPGR) (TR = 7.4 ms, TE = 3 ms, TI = 600, 10 degree flip angle, 25.6 cm² field of view, matrix = 256 x 256), and XETA (extended Echo Train Acquisition), which produced a series of contiguous T2-weighted images (TR = 2500 ms, TE = 80 ms, 25.6 cm² field of view). Both structural acquisitions resulted in 1 mm thick slices. Resting state fMRI data was collected using an EPI BOLD sequence, containing 200 repetitions of a high resolution EPI scan (96 x 96 in plane, 24 cm² field of view; 3 mm thickness, TR = 3000 ms, TE = 30, 39 slices) acquired over 10 min. During this protocol, subjects were asked to close their eyes, and while the magnet ran.

2.3. Data analysis

Gray matter was segmented into 77 anatomical regions of interest (ROIs) using a semi-automatic FreeSurfer software, as part of the Slicer3 environment (www.slicer.org). Parcellation into Brodmann areas by FreeSurfer is a standard/default procedure, and segmentation is performed based on anatomical/atlases priors; thus no selection process is necessary. The parcellation process is described elsewhere (Fischl et al., 2004) and provides results that are similarly sensitive to disease related changes as manual tracing (Morey et al., 2009). The resting-state fMRI data was processed as follows. The first 5 scans were discarded, and the sixth was used as a target for motion correction. All remaining scans were co-registered to this scan using rigid body alignment and slicing timing correction using FSL software.

Table 1

<table>
<thead>
<tr>
<th></th>
<th>SZ (n = 18)</th>
<th>NC (n = 18)</th>
<th>Independent samples t-test</th>
<th>P</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age (years)</td>
<td>41.58 ± 9.54</td>
<td>39.21 ± 10.84</td>
<td>36 – 0.715</td>
<td>0.479</td>
</tr>
<tr>
<td>Socioeconomic status (SES)*</td>
<td>3.37 ± 1.21</td>
<td>1.95 ± 0.71</td>
<td>36 – 4.419</td>
<td>0.001***</td>
</tr>
<tr>
<td>Parental SES*</td>
<td>2.47 ± 1.07</td>
<td>2.11 ± 1.15</td>
<td>36 – 1.021</td>
<td>0.314</td>
</tr>
<tr>
<td>Handedness</td>
<td>0.71 ± 0.24</td>
<td>0.80 ± 0.17</td>
<td>36 – 1.315</td>
<td>0.197</td>
</tr>
<tr>
<td>MME</td>
<td>28.63 ± 2.17</td>
<td>29.36 ± 0.63</td>
<td>31 – 1.211</td>
<td>0.235</td>
</tr>
</tbody>
</table>

Mean ± SD.  
* Higher scores indicated lower SES.  
** – statistically significant.
(Smith et al., 2004). The data was then spatially smoothed, using 6 mm Gaussian filter, and temporally low-pass filtered with 0.08 Hz cutoff. Finally, we removed global contributions to the time courses from the white matter, ventricles and the whole brain by using multivariate linear regression. The next step in data analysis involved non-rigid registration of the structural MRI to the fMRI space for each subject. fMRI connectivity analysis was performed as follows. For each pair of ROIs (2926 connections in total), we computed Pearson correlation coefficient between every pair of voxels in the two regions, applied a Fisher r-to-z transform to each correlation, and averaged these values. These measures served as our connectivity features for subsequent statistical analyses. We also assess the significance of prior clinical knowledge in a separate experiment by preselecting 16 brain structures (8 in each hemisphere), believed to play an important role in the pathophysiology of schizophrenia (based on literature search and previous reviews). These are the superior temporal gyrus, the rostral middle frontal gyrus (roughly corresponding to the dorsolateral prefrontal cortex), the hippocampus, the amygdala, the anterior cingulate gyrus, the posterior cingulate gyrus, the parahippocampal gyrus and the Heschl's gyrus. Since prior results in the schizophrenia literature suggest that these regions play a role in the disease, here we focus on the associated connections. This allows us to discard potentially noisy connections between irrelevant brain regions, which may bias the results. We consider only correlations between these regions and the rest of the ROIs in our analysis (1096 connections).

Once the correlation coefficients are estimated for each connection in each individual, we compute the Gini Importance of each connectivity feature based on a Random Forest analysis (Breiman, 2001). The Random Forest is an ensemble of decision tree classifiers that incorporates multiple levels of randomization. Each tree is grown using a random subset of training data (first level of randomization); each “decision node” is constructed by searching over a random subset of features, in our case, correlation measures (second level of randomization). The Random Forest derives a score for each feature, known as Gini Importance (GI), which summarizes its discriminative power. At each decision step (node) of the tree, the algorithm selects the feature/threshold pair, from a random subset, that maximizes the separability of the training data. We then average these scores across subsets of the data; hence, they would no survive multiple comparison correction.

3. Results

3.1. Schizophrenia group abnormalities

Schizophrenia patients exhibited increased functional connectivity between the medial parietal region, including the posterior cingulate gyrus, and the frontal lobe (pars triangularis and opercularis of the inferior frontal gyrus, and dorsolateral prefrontal cortex). This was true for both the full dataset and for the analysis based on the pre-selected brain regions. Along with the increased functional connectivity, abnormal schizophrenia connectivity pattern also included reduced functional connectivity between the same medial parietal region and the left temporal lobe (inferior temporal gyrus and amygdala). Again, same pattern and features were highlighted using both the full dataset and the selected features. In addition, the inter-hemispheric connectivity between the left and the right temporal regions expressed reduced functional connectivity in the selected features analysis only. Results of GI analysis are demonstrated in Figs. 3 and 4. Finally, when using GI scores and pre-selected group of features (regions) for predicting group membership, we achieved as high as 75% prediction accuracy in distinguishing between controls and schizophrenia subjects.

3.2. Clinical correlations

In addition to group comparison, in order to understand clinical implications of functional connectivity disruptions in schizophrenia, we also calculated correlation coefficients between clinical symptoms obtained from PANSS (Positive and Negative Syndrome Scale (Kay et al., 1987)) and individual functional connectivities that revealed group differences in our analysis. The functional connections that exhibited hyper-connectivity in the schizophrenia group (i.e., between the medial parietal and inferior frontal and dorsolateral prefrontal regions) were negatively correlated with patients’ scores on the Negative (social withdrawal rho = −0.47, P = 0.041) and General (anxiety rho = −0.50, P = 0.26, retardation rho = −0.49, P = 0.030 and attention −0.49, P = 0.029) subscales of the PANSS. Furthermore, the functional connections that exhibited hypo-connectivity in the schizophrenia group (i.e., between the medial parietal and temporal regions) were positively correlated with patients’ scores on the Positive subscales of the PANSS (delusions rho = 0.50, P = 0.028 and hallucinations rho = 0.54, P = 0.016).

Fig. 1. Implementation of a single decision tree in the Random Forest algorithm. \( \nu \) is a given decision node. \((f, \eta)\) are the feature and threshold pair used to create child nodes \( \nu_1 \), and \( \nu_2 \).
As discussed previously, the most frequently studied feature (network) identified in resting state fMRI data is the default mode network (DMN). According to various sources, it includes medial frontal (including anterior cingulate), parietal (including posterior cingulate, precuneus and inferior parietal) and medial temporal (including hippocampus) areas of the brain (Raichle et al., 2001; Greicius et al., 2003). The activation pattern (low-frequency fluctuations) within all the elements of this network seems to strongly correlate with each other, and network as a whole has been associated with spontaneous and task independent, internally generated thought processes (Fox et al., 2005). It is further believed that the activation within this network is actively suppressed during the cognitive tasks, and that the degree of this suppression correlates with task performance (semantic recognition and semantic priming) (Jeong and Kubicki, 2010). In schizophrenia, few similar observations have been made in relation to the task performance, i.e. Whitfield-Gabrieli et al. (2009) report anticorrelations between default-mode network and working memory performance, while Jeong and Kubicki (2010) report anticorrelations between default-mode network and semantic processes in schizophrenia. Both those studies suggest that the decreased activation and poorer cognitive performance in schizophrenia might be partially related to increased activation/decreased suppression within the default-mode network.

Both increased (Zhou et al., 2010) and decreased connectivity (Liang et al., 2006; Bluhm et al., 2007) in the default-mode network has been reported previously in patients with schizophrenia. The results of our study show that those previous results do not necessarily contradict each other. Instead, schizophrenia might, even at the level of each functional network, be associated with distinct patterns of functional connectivity abnormalities, in which certain connections (i.e., parietal–temporal and the temporal cortices bilaterally) have subnormal levels of functional connectivity while others (i.e., parietal–frontal) show supra-normal connectivity.

Increased levels of activation within the anterior part of the default network in schizophrenia (which also overlap with the brain regions involved in executive function and attention) could potentially interact with the posterior connections (i.e., tempo-parietal), thereby decreasing their effective connectivity and potentially affecting important cognitive processes that would rely on such connectivity, such as early auditory (Javitt et al., 1993), or semantic (Saykin et al., 1991; Nestor et al., 1993) processes. Furthermore, since the posterior and inferior temporal–parietal regions have been consistently implicated in the clinical symptoms of schizophrenia (specifically, in hallucinations and thought disorder (Woodruff et al., 1997), it is possible that the functional connectivity disruptions between these regions, such as observed in the present study, as well as their correlations with hallucinations and delusions also observed here, directly reflect
anatomical abnormalities reported in the literature, such as volume decreases in the STG, Heschl’s gyrus (associated with auditory hallucinations Barta et al., 1990), and the amygdala–hippocampus complex (associated with thought disorder Shenton et al., 2001) (for the review also see Niznikiewicz et al., 2003). The second possibility is that decreased anatomical connectivity between temporal and posterior parietal regions (implicated by anatomical DTI studies reporting abnormalities in white matter integrity in the cingulum bundle and arculate fasciculus (for the review, see Kubicki et al., 2007)), might decrease the inhibitory, “task related” input into the medial parietal region. This would further reflect in hyperactivation and hyperconnectivity within the frontal connections and attention deficits that are subserved by this connection, and are quite frequent in schizophrenia (as well as reflected by correlations with general and negative symptoms reported here). In addition to parieto-frontal and parieto-temporal connectivity abnormalities observed in our sample, our abnormal connectivity pattern also involved interhemispheric connections between temporal regions. Such abnormalities, despite being poorly understood, have been also suggested in multiple theories involving neurodevelopment and neurodegeneration in schizophrenia (Crow et al., 2007), and further suggest necessity of involving connections between the left and the right hemisphere in all experimental models of schizophrenia.

It is worth mentioning that while our analysis exhibits a distinct prediction power, unlike PCA approaches, the results do not imply that the important connections belong to the same functional network. Since not all schizophrenia patients share the same clinical manifestations, functional signal fluctuations should be more variable within this group than within healthy controls. Our method is designed to find connections that consistently and together differentiate patients and controls. Accordingly, in our previous, methodological publication (Venkataraman et al., 2010), we demonstrated that Gini Importance, as opposed to univariate scores, remains consistent across cross-validation iterations, and significant connectivity features have reasonable predictive power in distinguishing those populations. We notice, however, that in the current experiment, a small subset of subjects is consistently misclassified. This suggests that functional connectivity differences between two populations are quite subtle. Additionally, since resting functional connectivity is not a well-understood phenomenon, the results may be confounded by external factors, which include anatomical variability in “white matter connectivity”, age, medication levels, etc. Once fully understood, accounting for these factors might vastly improve analytic power of functional connectivity experiments. It is worth recalling, however, that not only is schizophrenia a clinically inhomogeneous disease, but various anatomical and/or physiological disturbances might lead to the same clinical manifestation. This renders

![Brain Connectivity Diagrams](image-url)
the search for a schizophrenia phenotype even more complex and difficult.

Role of funding source
This study was supported, in part, by the National Alliance for Medical Image Computing (NA-MIC), supported through the National Institutes of Health Roadmap for Medical Research, Grant U54 EB005149 (MK, CFW, PG); and National Institute of Health (ROI M074794 to CFW and MK). This work was also supported by a grant from the Medical Research Council of Australia (Overseas-Based Biomedical Training Fellowship (NHMRC 520627), through the Melbourne Neuro-Psychiatry Centre at the University of Melbourne, to TJW). A Venkataraman was supported by the National Defense Science and Engineering Graduate Fellowship.

Contributors
A. Venkataraman designed the study and ran the analyses. Dr Kubicki provided fMRI data. Drs Kubicki, Golland and Westin supervised various aspects of the study. Dr Whitford undertook clinical statistical analyses, Drs Kubicki and Whitford helped interpreting clinical findings, and A. Venkataraman wrote the first draft of the manuscript. All authors contributed to and have approved the final manuscript.

Conflict of interest
The authors report no conflict of interests.

Acknowledgments
We want to thank PNL research assistants (Jorge Alvarado and Tali Swisher) for their help with data organization and endnote libraries.

References